

# Towards Real-Time Bayesian Inference for Magnetoencephalography

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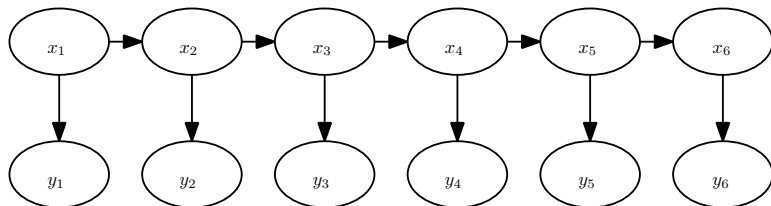
# Outline

- ▶ Background
  - ▶ Magnetoencephalography
  - ▶ Hidden Markov Models / State Space Models
  - ▶ Particle Filters / Sequential Monte Carlo
- ▶ Models for Filtering of MEG Data
- ▶ Examples
- ▶ Computational Considerations
- ▶ Conclusions

# Magnetoencephalography

- ▶ Noninvasive imaging technique which measures magnetic fields induced by neural currents.
- ▶ Sampling rate  $\sim 100\text{Hz}$ .
- ▶ Ill-posed inverse problem: turn measurements into estimates of brain activity.
- ▶ Problem addressed: estimation of current brain activity given observations received.

# Hidden Markov Models



- ▶ Unobserved Markov chain  $\{X_n\}$  transition  $f$ .
- ▶ Observed process  $\{Y_n\}$  conditional density  $g$ .
- ▶ Density:

$$p(x_{1:n}, y_{1:n}) = f_1(x_1)g(y_1|x_1) \prod_{i=2}^n f(x_i|x_{i-1})g(y_i|x_i).$$

# Formal Solutions

- ▶ Filtering and Prediction Recursions:

$$p(x_n|y_{1:n}) = \frac{p(x_n|y_{1:n-1})g(y_n|x_n)}{\int p(x'_n|y_{1:n-1})g(y_n|x'_n)dx'_n}$$

$$p(x_{n+1}|y_{1:n}) = \int p(x_n|y_{1:n})f(x_{n+1}|x_n)dx_n$$

- ▶ Smoothing:

$$p(x_{1:n}|y_{1:n}) = \frac{p(x_{1:n-1}|y_{1:n-1})f(x_n|x_{n-1})g(y_n|x_n)}{\int g(y_n|x'_n)f(x'_n|x_{n-1})p(x'_{n-1}|y_{1:n-1})dx'_{n-1:n}}$$

## Importance Sampling in This Setting

- ▶ Given  $p(x_{1:n}|y_{1:n})$  for  $n = 1, 2, \dots$
- ▶ Could sample from a sequence  $q_1(x_1), \dots, q_n(x_{1:n})$
- ▶ If  $q_n(x_{1:n}) = q_n(x_n|x_{1:n-1})q_{n-1}(x_{1:n-1})$   
we can re-use samples.
- ▶ Weight:

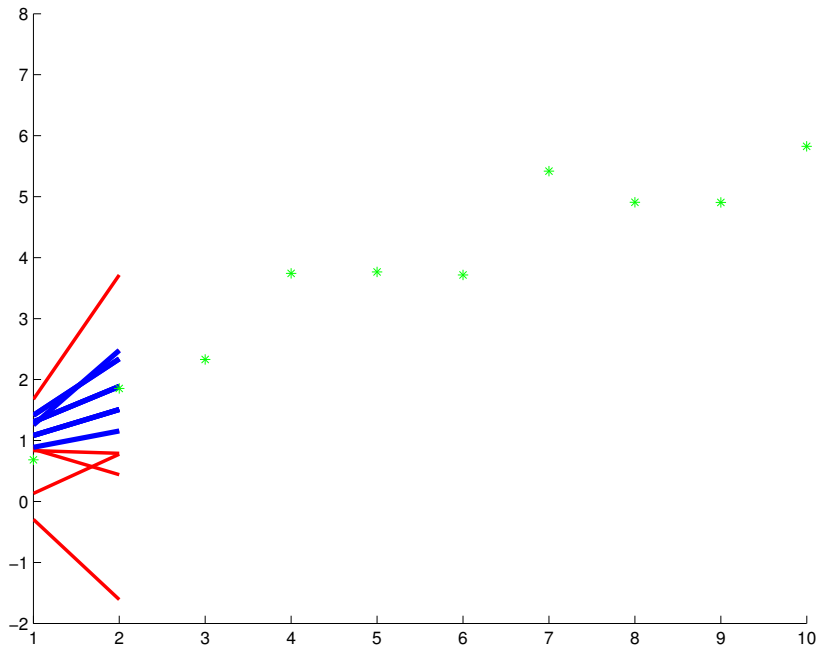
$$\begin{aligned}w_n(x_{1:n}) &\propto \frac{p(x_{1:n}|y_{1:n})}{q_n(x_n|x_{1:n-1})q_{n-1}(x_{1:n-1})} \\ &= \frac{p(x_{1:n}|y_{1:n})}{q_n(x_n|x_{1:n-1})p(x_{1:n-1}|y_{1:n-1})} w_{n-1}(x_{1:n-1}) \\ &= \frac{f(x_n|x_{n-1})g(y_n|x_n)}{q_n(x_n|x_{n-1})p(y_n|y_{1:n-1})} w_{n-1}(x_{1:n-1})\end{aligned}$$

# SIR Particle Filters [GSS93]

Can be viewed as an extension of importance sampling

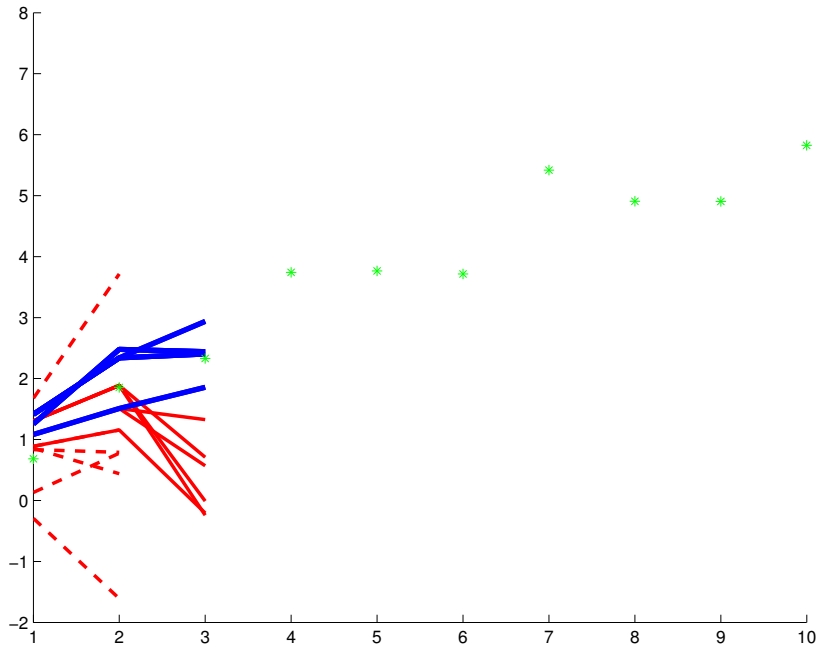
- ▶ Algorithmically, at iteration  $n$ :
  - ▶ Given  $\{W_{n-1}^i, X_{1:n-1}^i\}$  for  $i = 1, \dots, N$ :
  - ▶ **Resample**, obtaining  $\{1/N, \tilde{X}_{1:n-1}^i\}$ .
    - ▶ Sample  $X_n^i \sim q_n(\cdot | \tilde{X}_{n-1}^i)$
    - ▶ Weight  $W_n^i \propto \frac{f(X_n^i | \tilde{X}_{n-1}^i) g(y_n | X_n^i)}{q_n(X_n^i | \tilde{X}_{n-1}^i)}$
- ▶ Actually:
  - ▶ Resample efficiently.
  - ▶ Only resample when necessary.

## Iteration 2

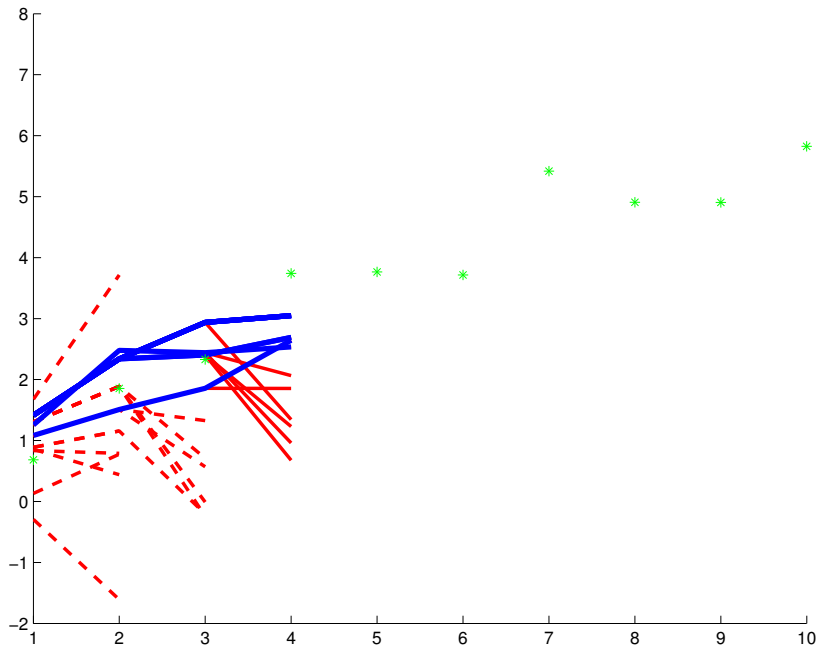




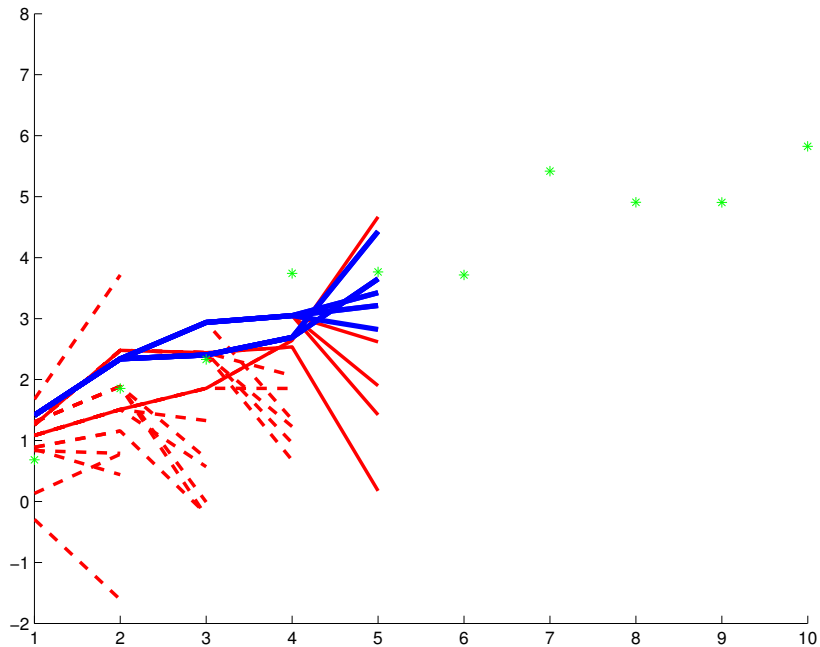
# Iteration 3



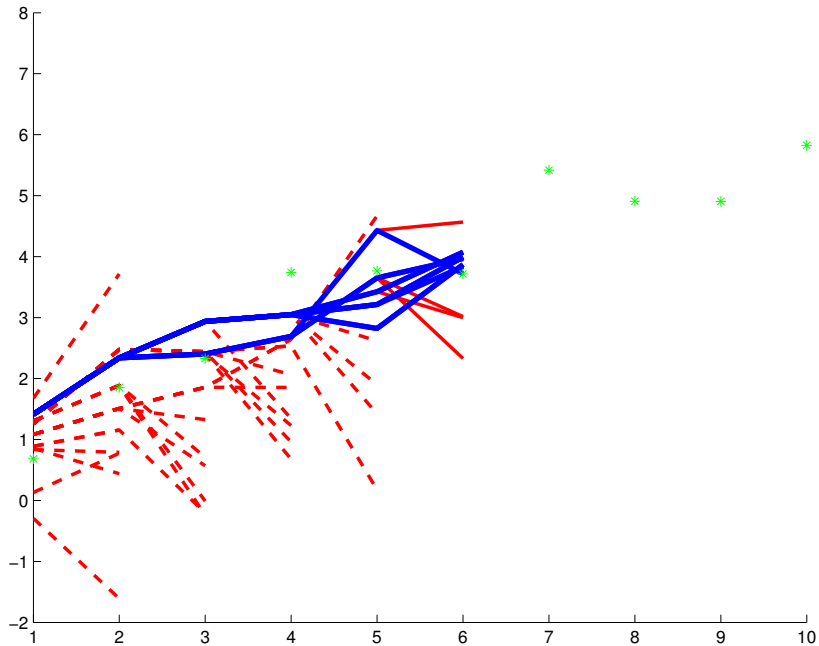
# Iteration 4



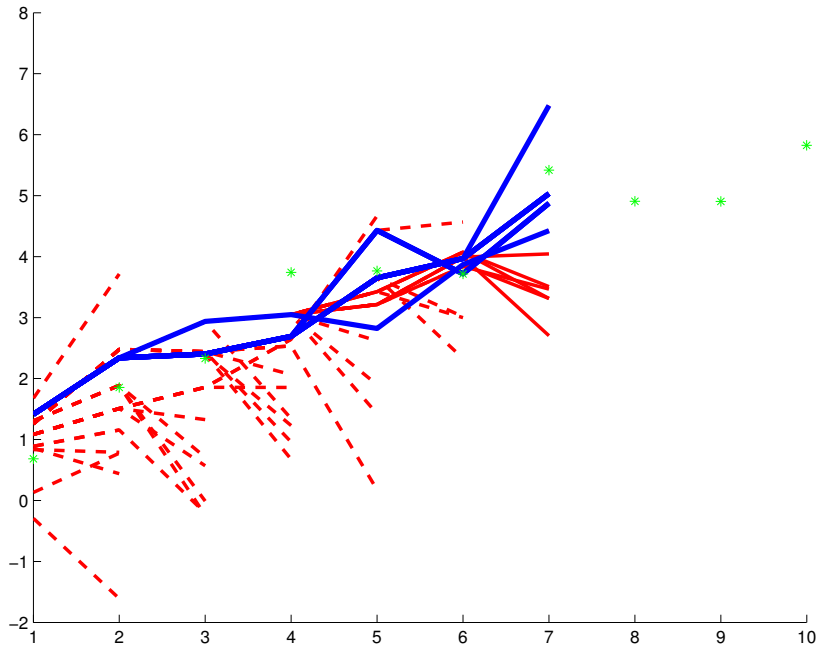
# Iteration 5



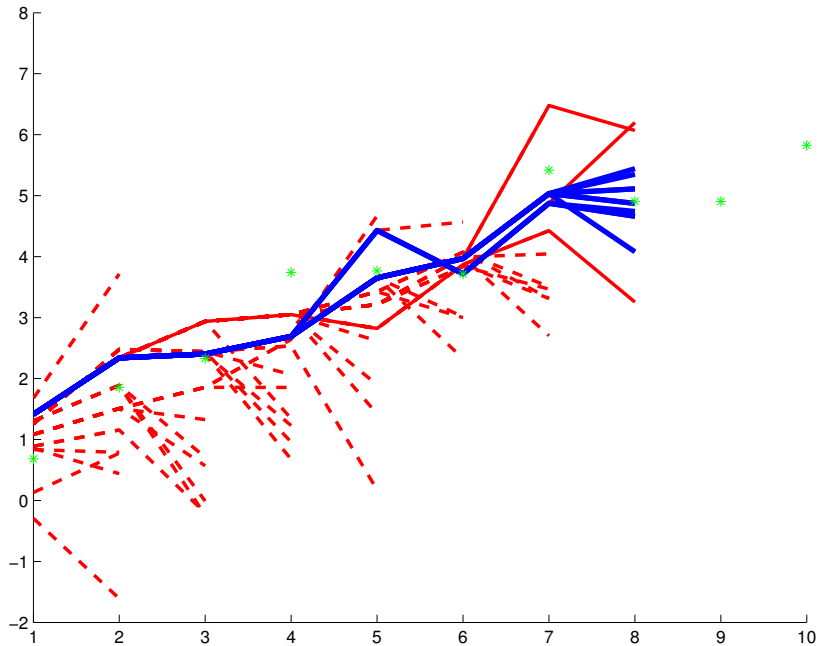
# Iteration 6



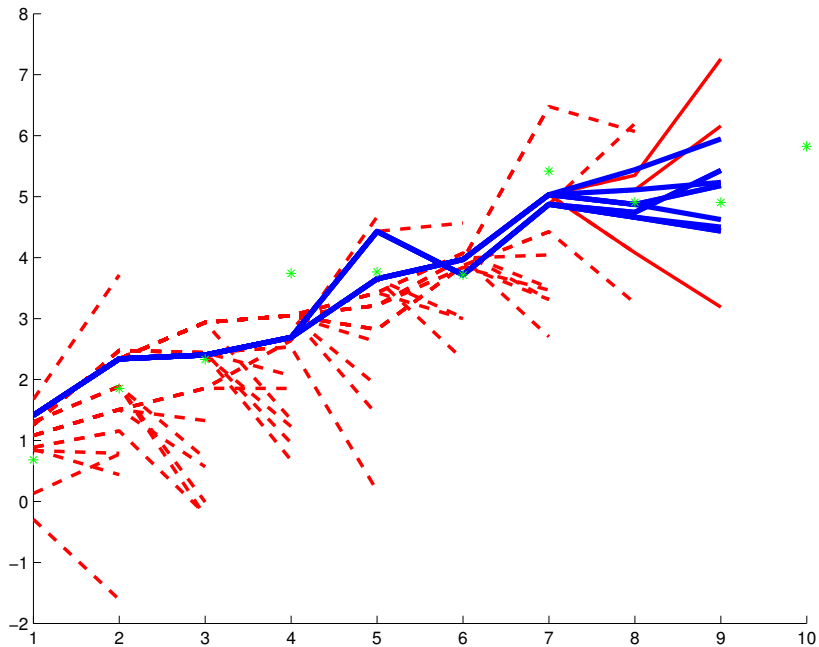
# Iteration 7



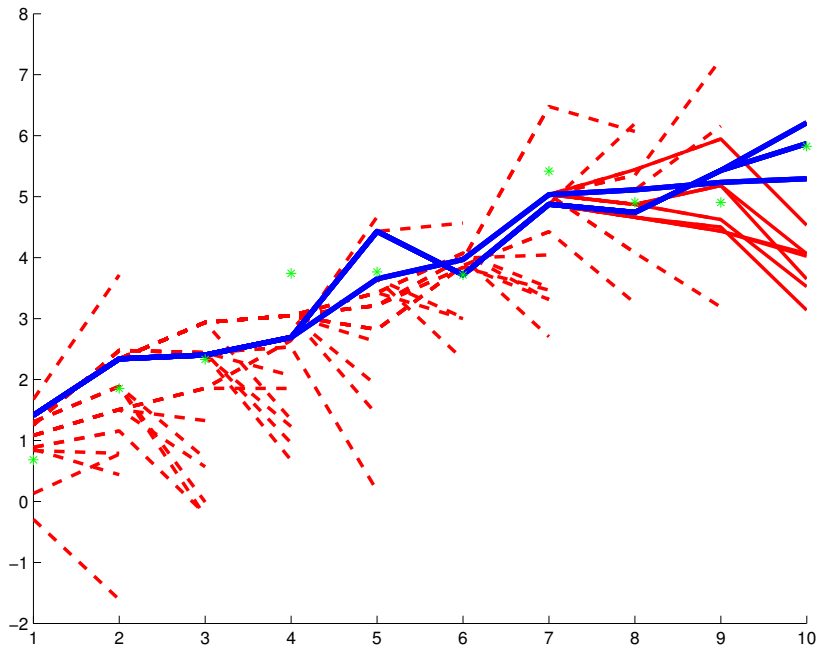
# Iteration 8



# Iteration 9



# Iteration 10





## Resample-Move Particle Filters [GB01]

- ▶ Originally, incorporate  $p(x_t|y_{1:t})$ -invariant MCMC kernels.
- ▶ Here we consider  $p(x_{1:t}|y_{1:t})$ -invariant kernels.
- ▶ Actually, go back only to the birth of the oldest surviving dipole.

## Measurement Model

- ▶ Work with discretized brain ( $N_{\text{grid}} \approx 10000$  elements).
- ▶ Precompute ( $N_{\text{sensors}} \times 3N_{\text{grid}}$ ) leadfield/gain matrix,  $G$ .

$$p(b_t | j_t) = \mathcal{N} \left( b_t; \sum_{i=1}^{N_t} G \left( r_t^{(i)} \right) q_t^{(i)}, \Sigma_{\text{noise}} \right)$$

where

$$j_t = \left( \left( r_t^{(1)}, q_t^{(1)} \right), \dots, \left( r_t^{(N_t)}, q_t^{(N_t)} \right) \right)$$

and  $G(r)$  is a  $N_{\text{sensors}} \times 3$  matrix for each  $r$ .

# A Random Walk with Births and Deaths

Mixture of 3 components:

$$p(j_t | j_{t-1}) = P_{\text{birth}}(j_{t-1}) T_{\text{birth}}(j_t | j_{t-1}) + \\ P_{\text{death}}(j_{t-1}) T_{\text{death}}(j_t | j_{t-1}) + \\ P_{\text{rw}}(j_{t-1}) T_{\text{rw}}(j_t | j_{t-1})$$

Where:

$$T_{\text{birth}}(j_t | j_t) = T_{\text{rw}}(j_t^{(1:N_{t-1})} | j_{t-1}) U_{\text{grid}}(r_t^{(N_{t-1}+1)}) \mathcal{N}(q_t^{(N_{t-1}+1)}; 0, \sigma_q I)$$
$$T_{\text{death}}(j_t | j_t) = \frac{1}{N_{t-1}} \sum_{i=1}^{N_{t-1}} T_{\text{rw}}(j_t | j_{t-1} \setminus (r_{t-1}^{(i)}, q_{t-1}^{(i)}))$$
$$T_{\text{rw}}(j_t | j_t) = \prod_{i=1}^{N_{t-1}} \mathcal{N}|_{\text{grid}}(r_t^{(i)}; r_{t-1}^{(i)}) \mathcal{N}(q_t^{(i)}; q_{t-1}^{(i)}, \Delta)$$

# A Static Dipole Model [SJA<sup>+</sup>13]

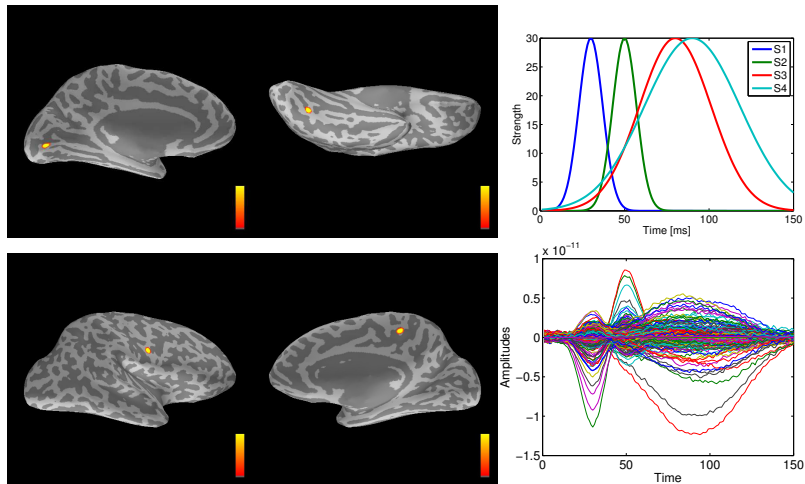
Mixture of 3 components:

$$p(j_t | j_{t-1}) = P_{\text{birth}}(j_{t-1})T_{\text{birth}}(j_t | j_{t-1}) + \\ P_{\text{death}}(j_{t-1})T_{\text{death}}(j_t | j_{t-1}) + \\ P_{\text{sd}}(j_{t-1})T_{\text{sd}}(j_t | j_{t-1})$$

Where:

$$T_{\text{birth}}(j_t | j_t) = T_{\text{sd}}(j_t^{(1:N_{t-1})} | j_{t-1}) U_{\text{grid}}(r_t^{(N_{t-1}+1)}) \mathcal{N}(q_t^{(N_{t-1}+1)}; 0, \sigma_q I)$$
$$T_{\text{death}}(j_t | j_t) = \frac{1}{N_{t-1}} \sum_{i=1}^{N_{t-1}} T_{\text{sd}}(j_t | j_{t-1} \setminus (r_{t-1}^{(i)}, q_{t-1}^{(i)}))$$
$$T_{\text{sd}}(j_t | j_t) = \prod_{i=1}^{N_{t-1}} \delta_{r_{t-1}^{(i)}}(r_t^{(i)}) \mathcal{N}(q_t^{(i)}; q_{t-1}^{(i)}, \Delta)$$

# Simulation Experiment



Source locations (top row S1 and S2, bottom row S3 and S4), source time courses and generated noisy field.

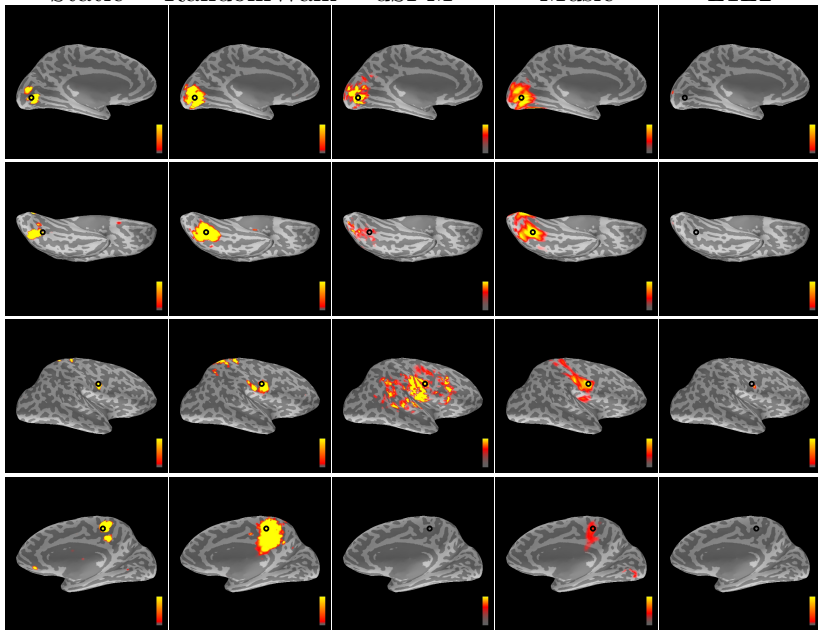
Static

RandomWalk

dSPM

Music

L1L2



## Application to Real Data

- ▶ Somatosensory Evoked Fields mapping experiment
- ▶ Acquired with 306-channel MEG device [204 planar gradiometers; 102 magnetometers]
- ▶ The left median nerve at wrist was electrically stimulated at the motor threshold (interstimulus interval randomly varying between 7.0 s and 9.0 s).
- ▶ Signals filtered to 0.1-200 Hz and sampled at 1000 Hz.
- ▶ Electrooculogram (EOG) used to monitor eye movements.
- ▶ Trials with EOG or MEG exceeding 150 mV or 3 pT/cm were excluded.
- ▶ 84 clean trials were averaged.
- ▶ To reduce external interference, signal space separation method was applied to the average.
- ▶ A 3D digitizer and four head position indicator coils were employed to determine the position of the subject's head.

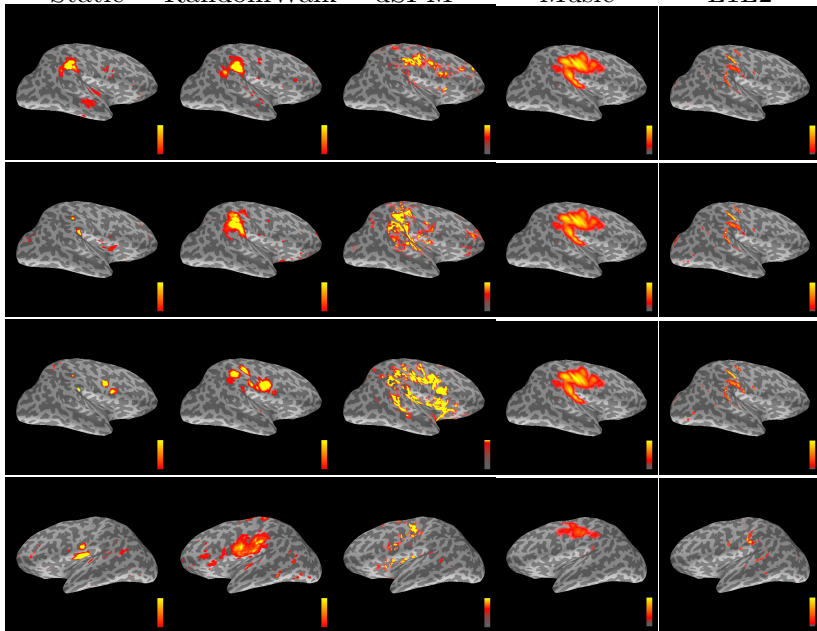
Static

RandomWalk

dSPM

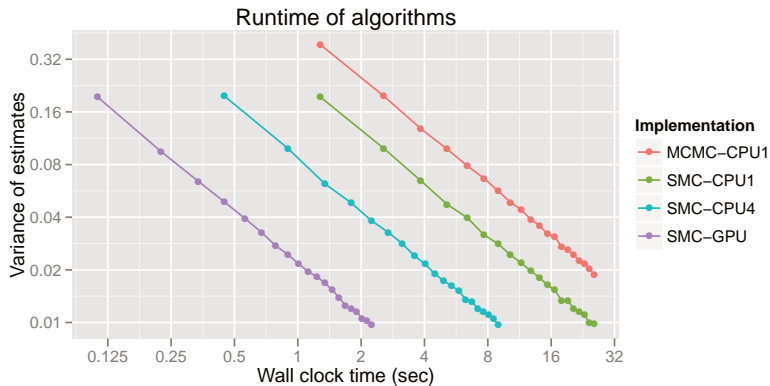
Music

L1L2





# Computational Considerations: A Related PET Algorithm [ZJA15]



# Conclusions

- ▶ Modelling and computational considerations interact.
- ▶ Static dipole models allow better interpretation.
- ▶ Online inference under such models is possible with care.
- ▶ Computational costs are manageable...
- ▶ and parallelisation is easy.

# References



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